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Mahoney et al.

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(54) **SYSTEMS AND METHODS FOR SPINAL SURGERY**

USPC 606/86 A, 86 B, 99
See application file for complete search history.

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(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 853 days.

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(21) Appl. No.: **13/185,775**

Brantigan, J. et al., "Posterior Lumbar Interbody Fusion Technique Using the Variable Screw Placement Spinal Fixation System," Spine: State of the Art Reviews, 6(1):175-200 (Jan. 1992).

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(65) **Prior Publication Data**

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Related U.S. Application Data

Primary Examiner — Nicholas Woodall

(62) Division of application No. 10/579,146, filed as application No. PCT/US2005/004136 on Feb. 9, 2005, now Pat. No. 8,016,829.

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(60) Provisional application No. 60/543,030, filed on Feb. 9, 2004.

(57) **ABSTRACT**

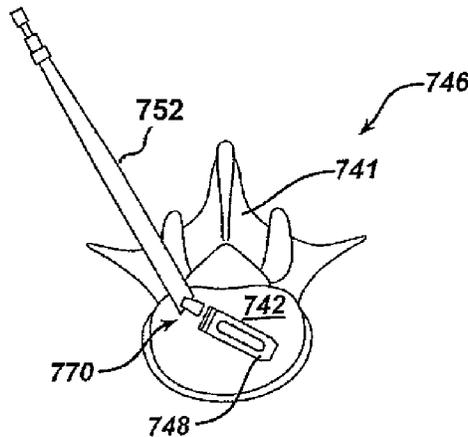
Disclosed herein are methods and devices for distracting adjacent vertebrae during surgical procedures for implanting spinal prostheses. In an exemplary embodiment, a distractor is disclosed that maintains the empty space between adjacent vertebrae following a discectomy, and that can removably mate with other surgical instruments, such as, for example, a filler bar, an implanting tool, or a funnel. In other embodiments of the present invention a distractor is disclosed having various features to assist in implanting a spinal prosthesis, such as, for example, an angled distal end and/or an expandable paddle. In another embodiment of the present invention, an articulating inserter is disclosed. Moreover, various implants and funnels are also disclosed herein.

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A61B 17/56 (2006.01)
A61F 2/46 (2006.01)
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(52) **U.S. Cl.**
CPC **A61F 2/4611** (2013.01); **A61B 17/025** (2013.01); **A61F 2/447** (2013.01);
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(58) **Field of Classification Search**
CPC A61F 2/4611

9 Claims, 25 Drawing Sheets



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A61F 2/28 (2006.01)
A61F 2/30 (2006.01)

(52) **U.S. Cl.**
 CPC *A61F 2/4601* (2013.01); *A61B 2017/0256*
 (2013.01); *A61F 2/28* (2013.01); *A61F 2/30965*
 (2013.01); *A61F 2002/3038* (2013.01); *A61F*
2002/3052 (2013.01); *A61F 2002/30062*
 (2013.01); *A61F 2002/30092* (2013.01); *A61F*
2002/30112 (2013.01); *A61F 2002/30133*
 (2013.01); *A61F 2002/30217* (2013.01); *A61F*
2002/30235 (2013.01); *A61F 2002/30266*
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2002/30471 (2013.01); *A61F 2002/30476*
 (2013.01); *A61F 2002/30538* (2013.01); *A61F*
2002/30566 (2013.01); *A61F 2002/30772*
 (2013.01); *A61F 2002/30795* (2013.01); *A61F*
2002/30841 (2013.01); *A61F 2002/30904*
 (2013.01); *A61F 2002/4415* (2013.01); *A61F*
2002/4622 (2013.01); *A61F 2002/4627*
 (2013.01); *A61F 2002/4628* (2013.01); *A61F*
2210/0004 (2013.01); *A61F 2210/0014*
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2220/0033 (2013.01); *A61F 2220/0075*
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2230/0004 (2013.01); *A61F 2230/0015*
 (2013.01); *A61F 2230/0067* (2013.01); *A61F*
2230/0069 (2013.01); *A61F 2230/0082*
 (2013.01); *A61F 2250/0006* (2013.01); *A61F*
2310/00017 (2013.01); *A61F 2310/00023*
 (2013.01); *A61F 2310/00029* (2013.01); *A61F*
2310/00131 (2013.01); *A61F 2310/00359*
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FIG. 1

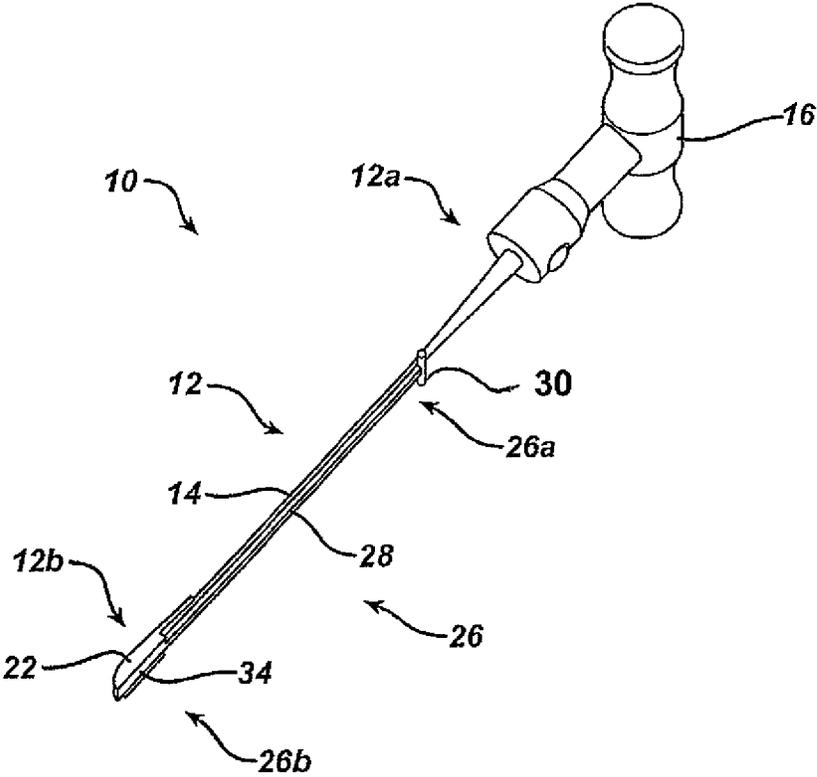


FIG. 2

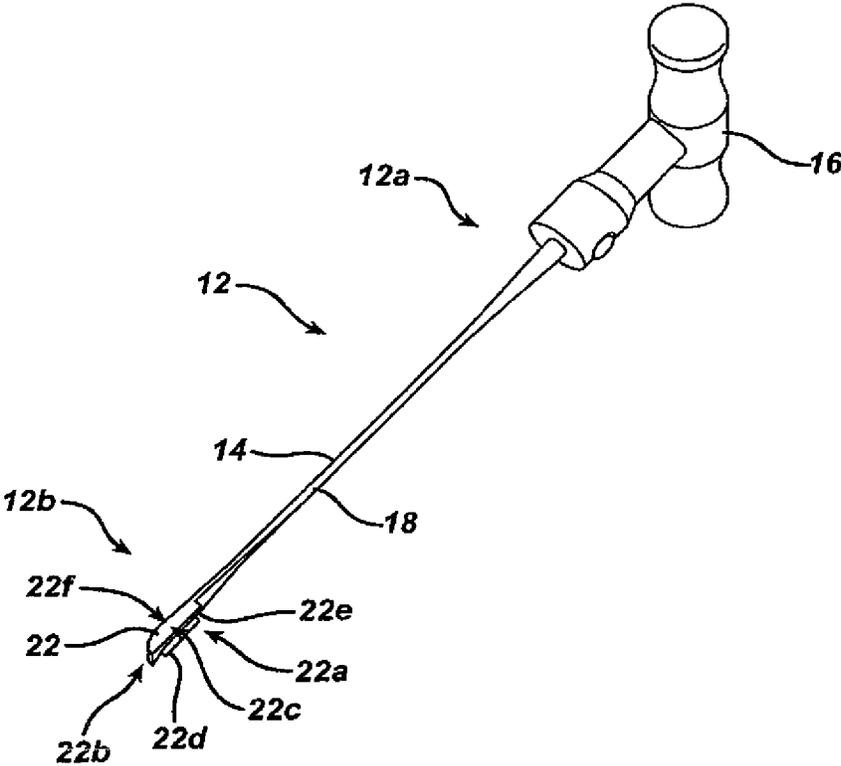


FIG. 3

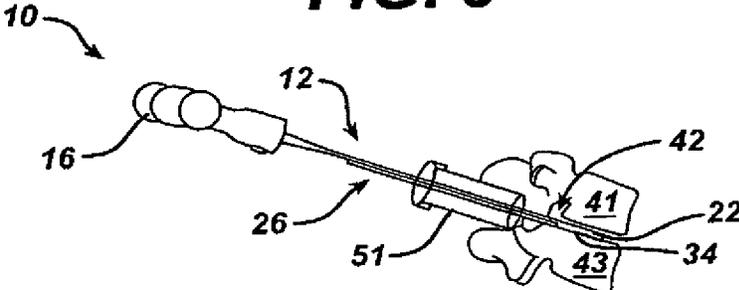


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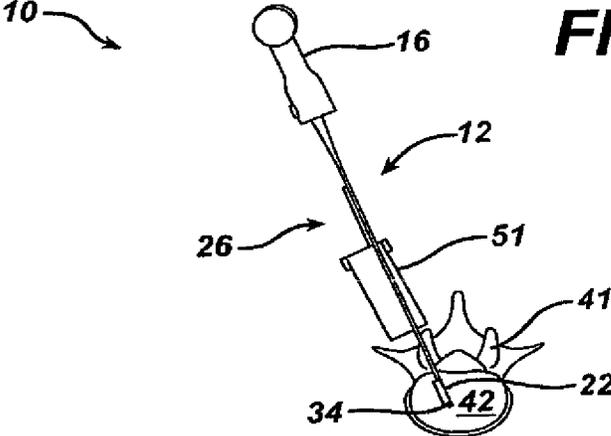


FIG. 5

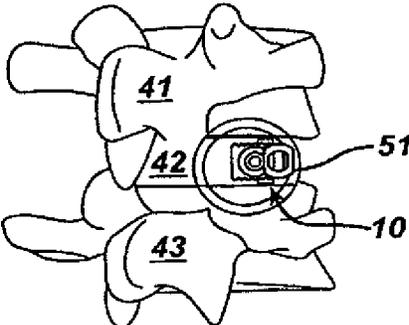
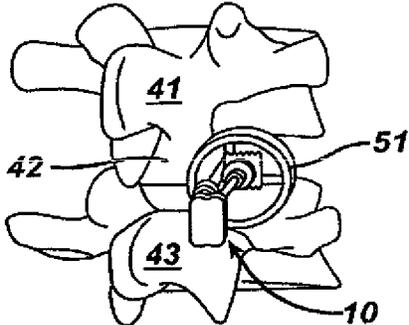
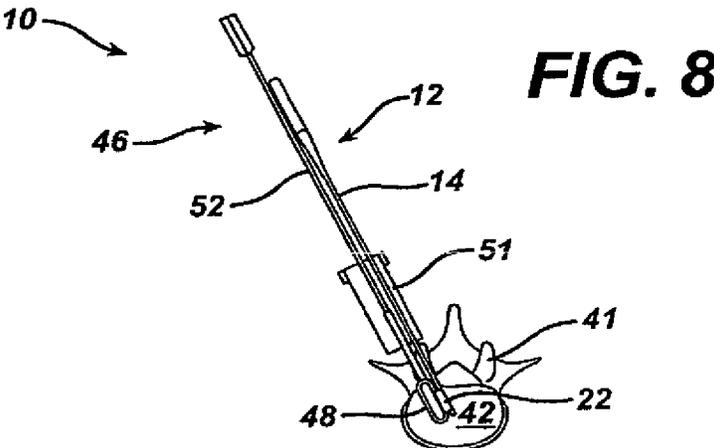
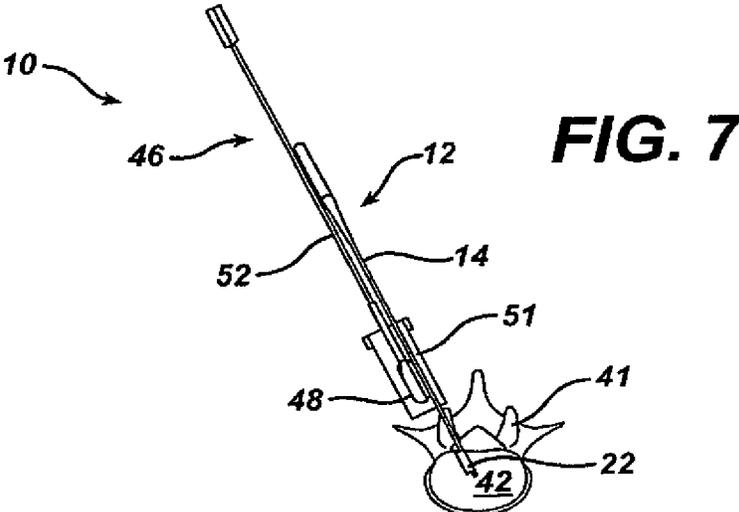


FIG. 6





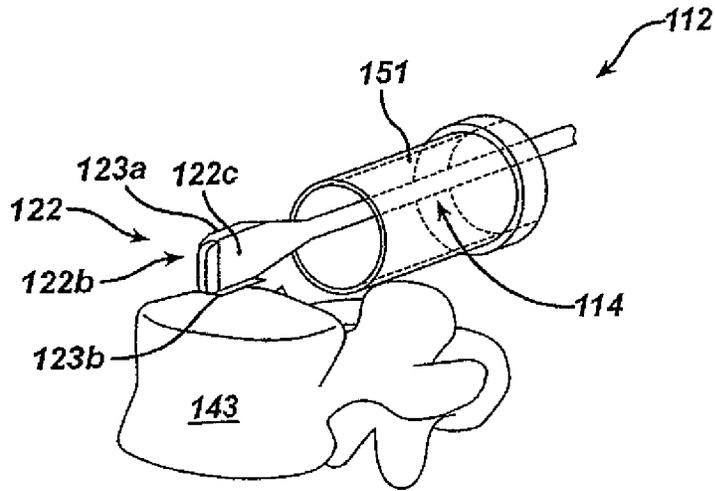


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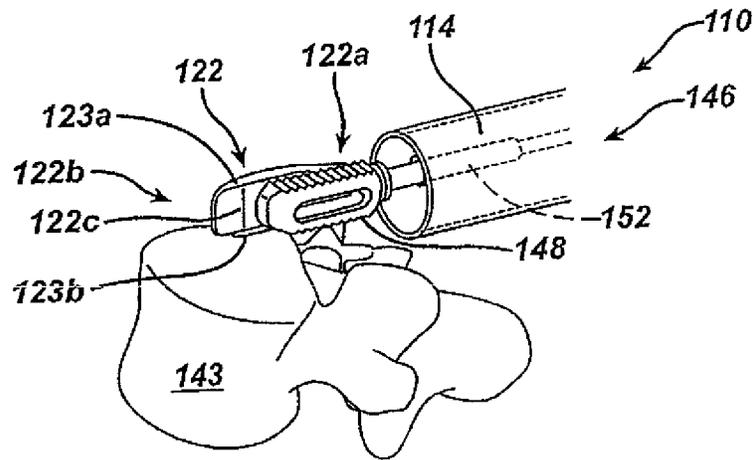


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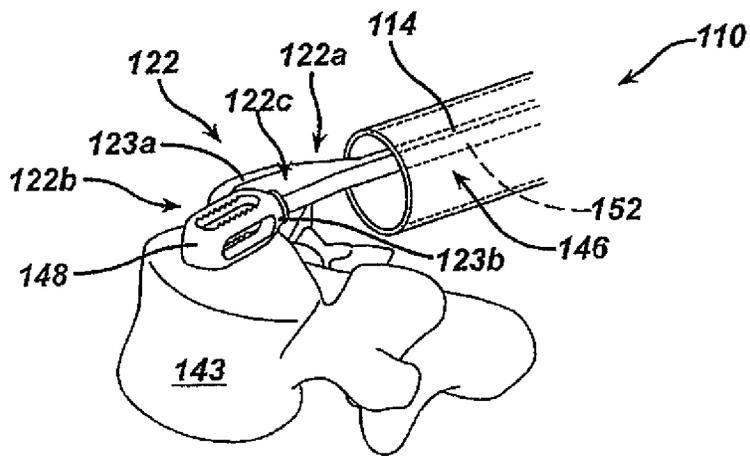


FIG. 11

FIG. 12

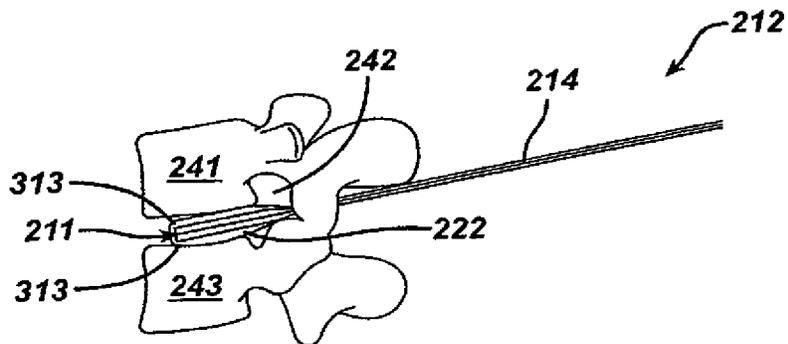
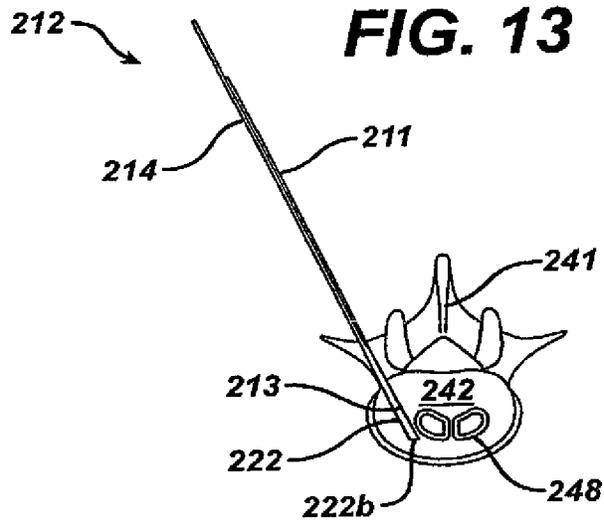


FIG. 13



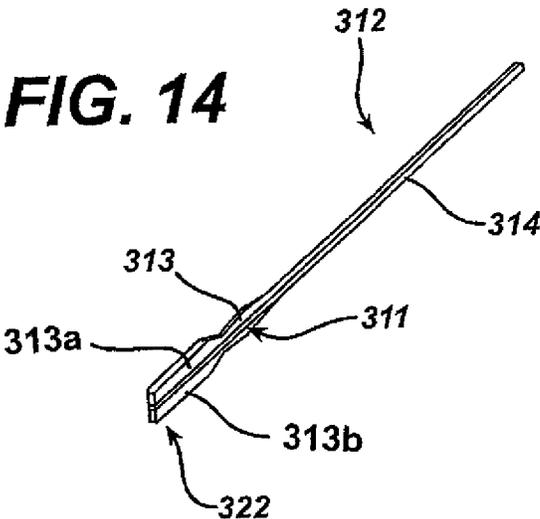


FIG. 15

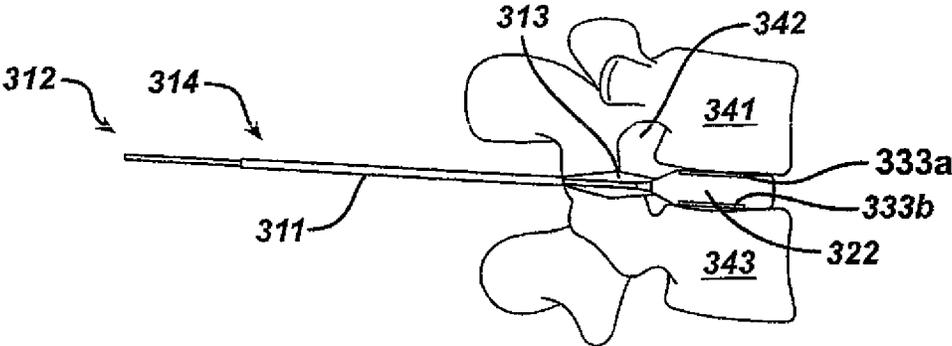


FIG. 16

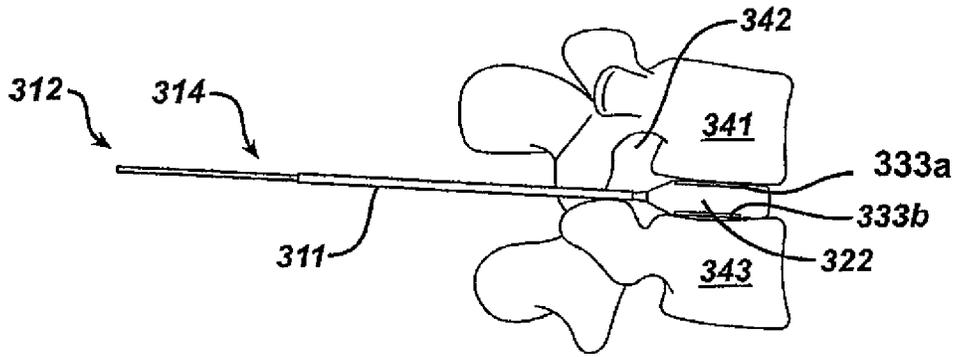
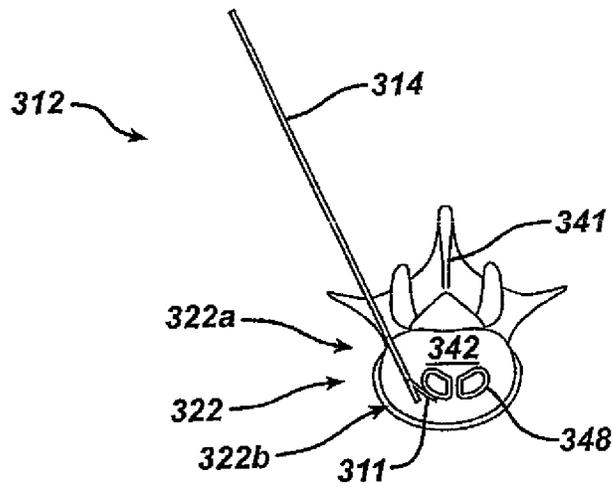


FIG. 17



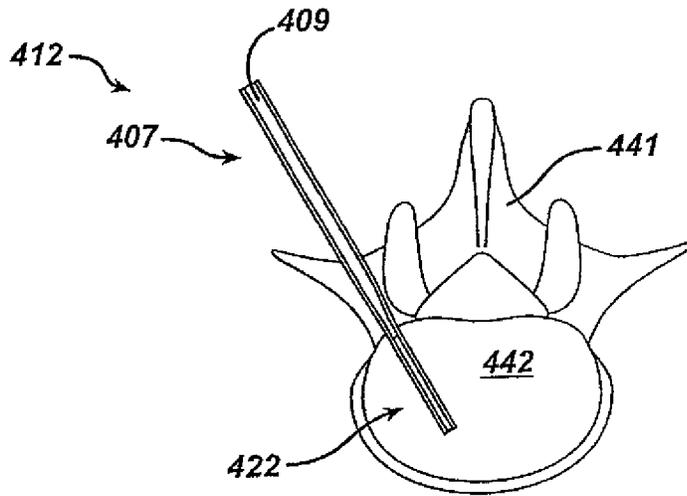


FIG. 18

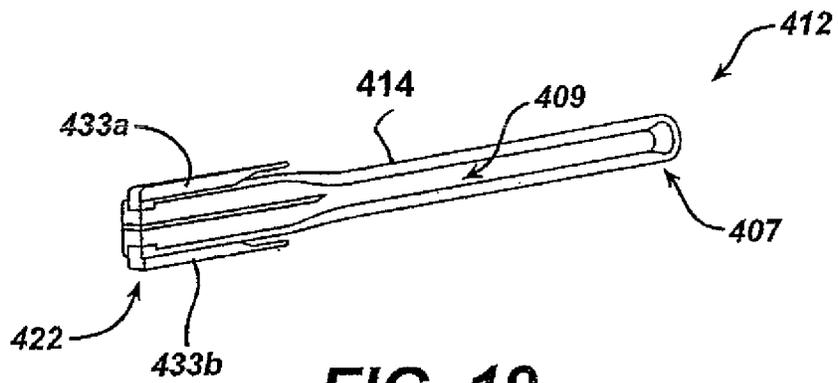


FIG. 19

FIG. 20

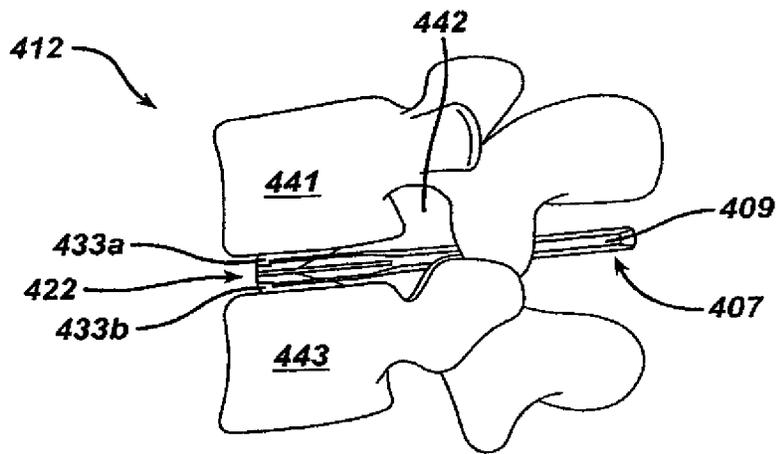


FIG. 21

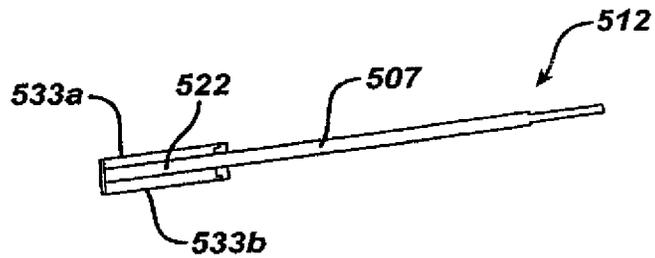


FIG. 22

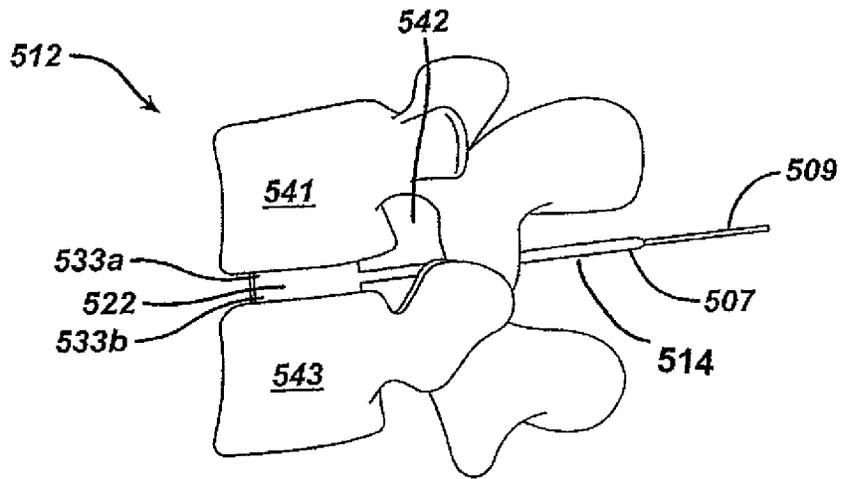


FIG. 23

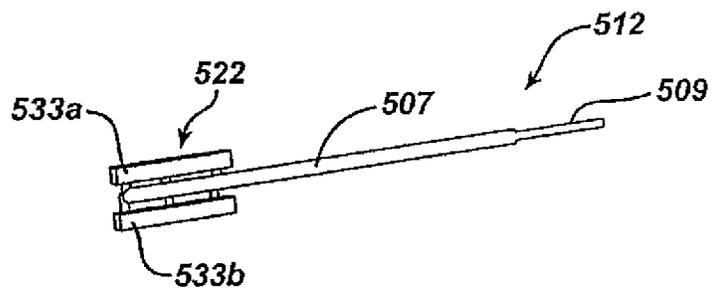


FIG. 24

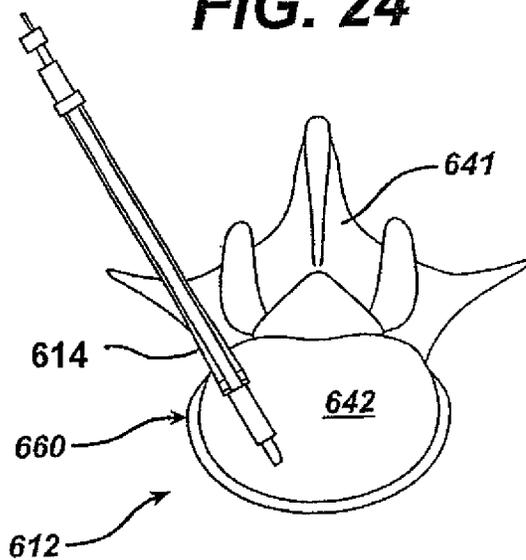


FIG. 25

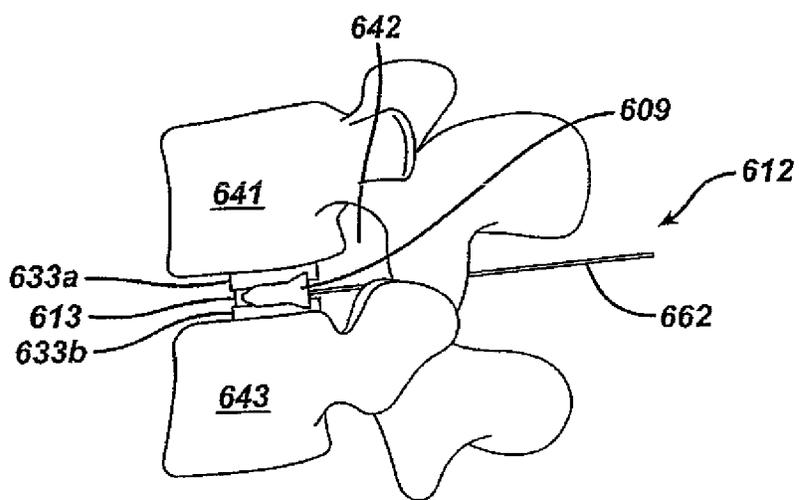


FIG. 26

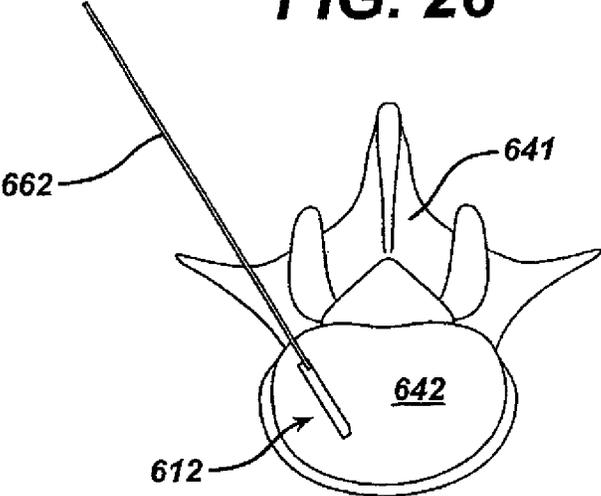


FIG. 27

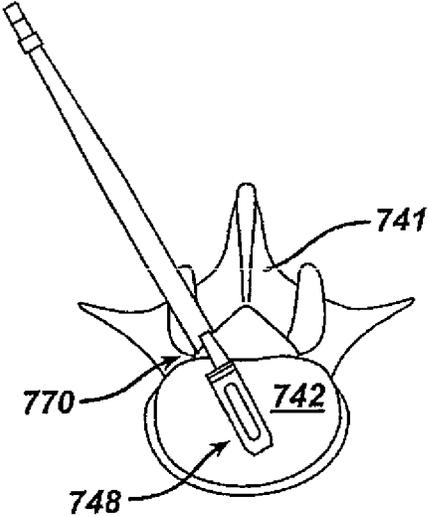


FIG. 28

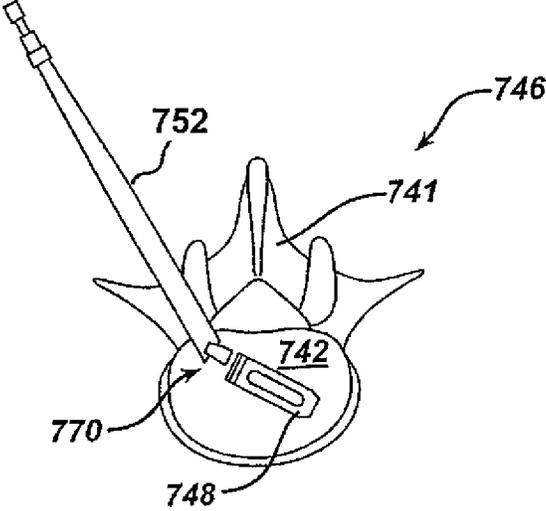
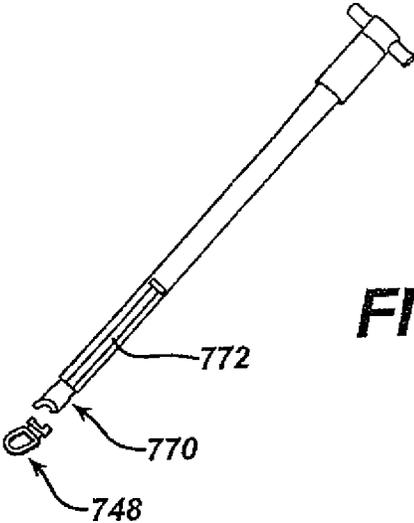
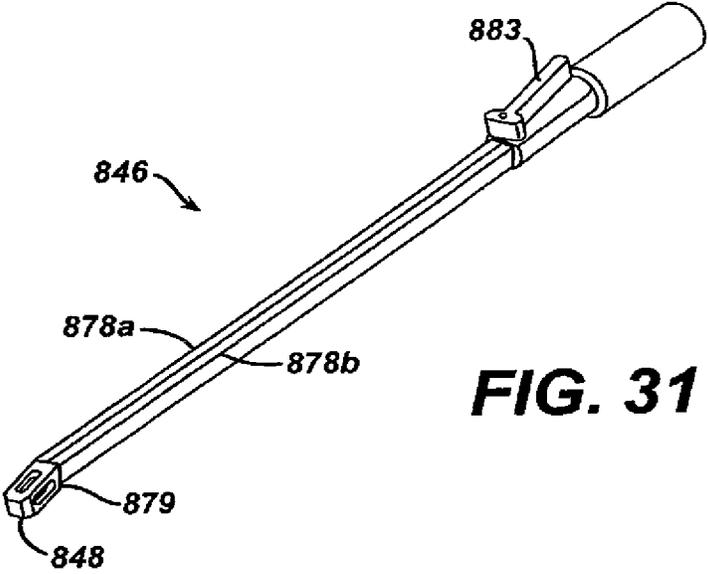
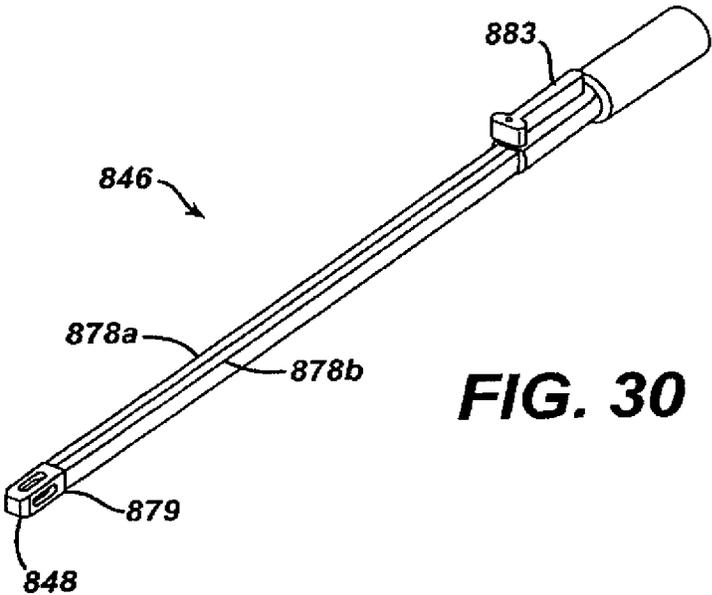
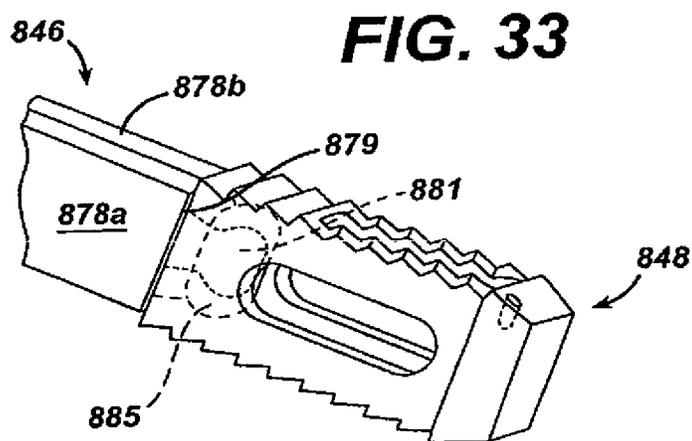
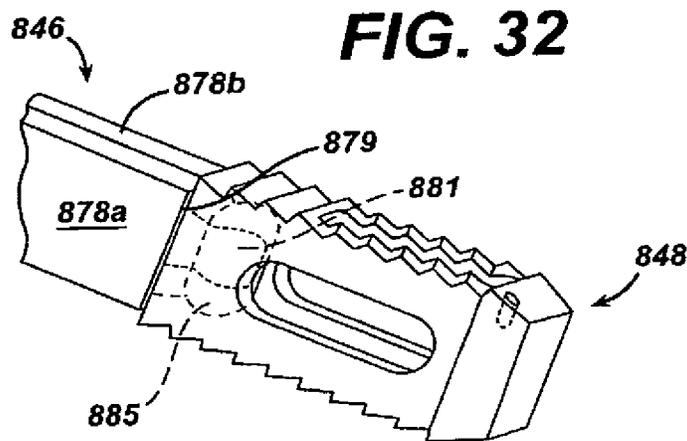


FIG. 29







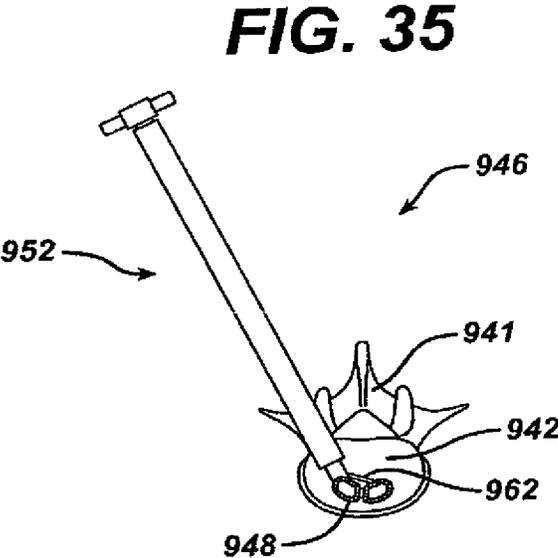
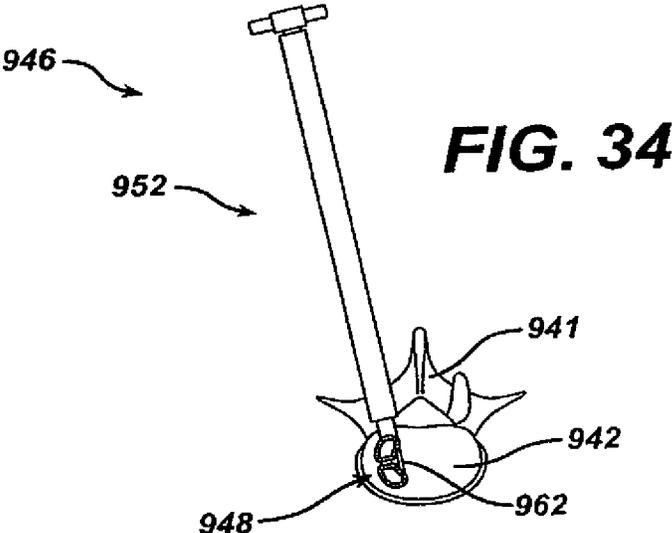


FIG. 36

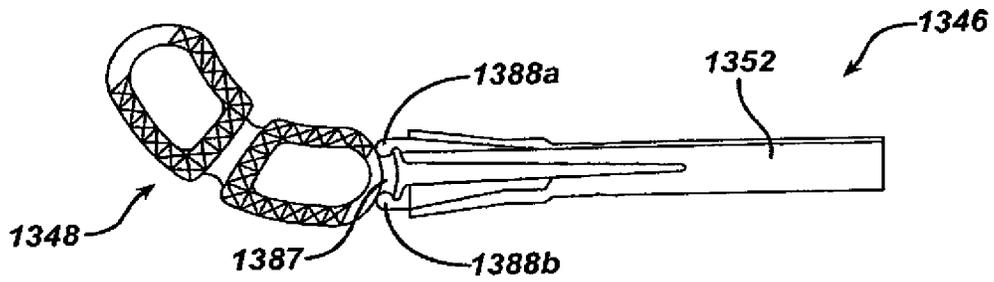


FIG. 37

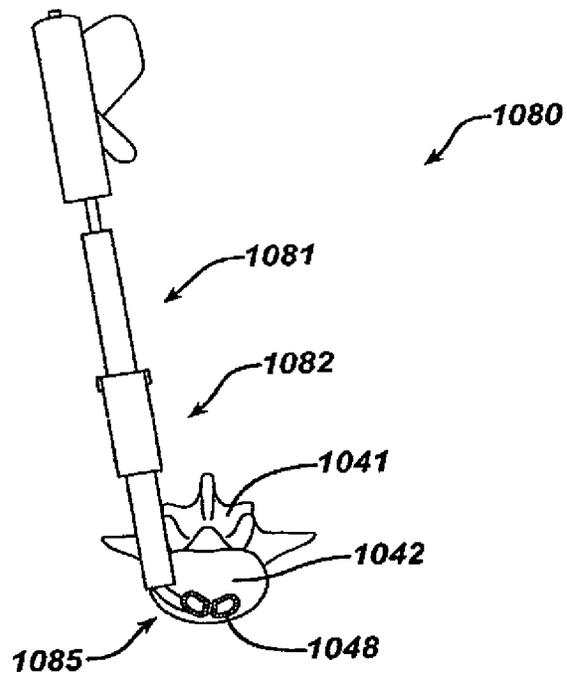


FIG. 38

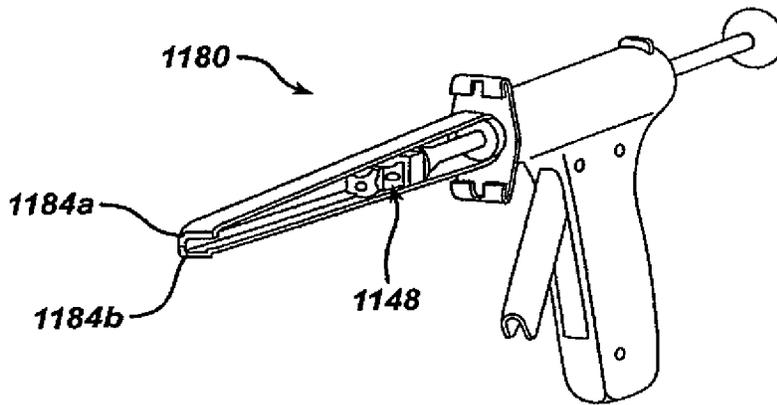


FIG. 39

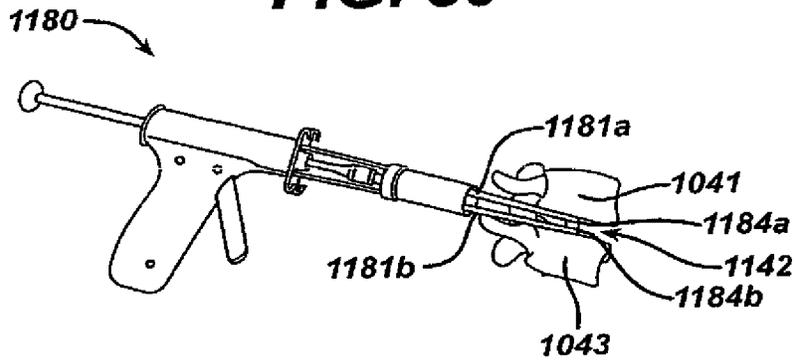


FIG. 40

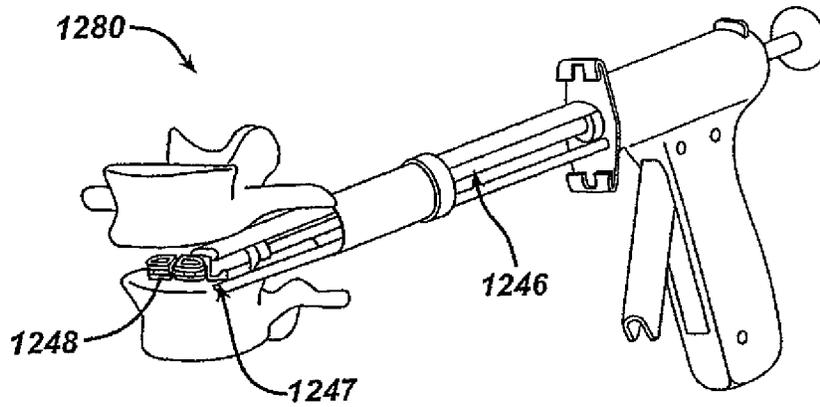


FIG. 41

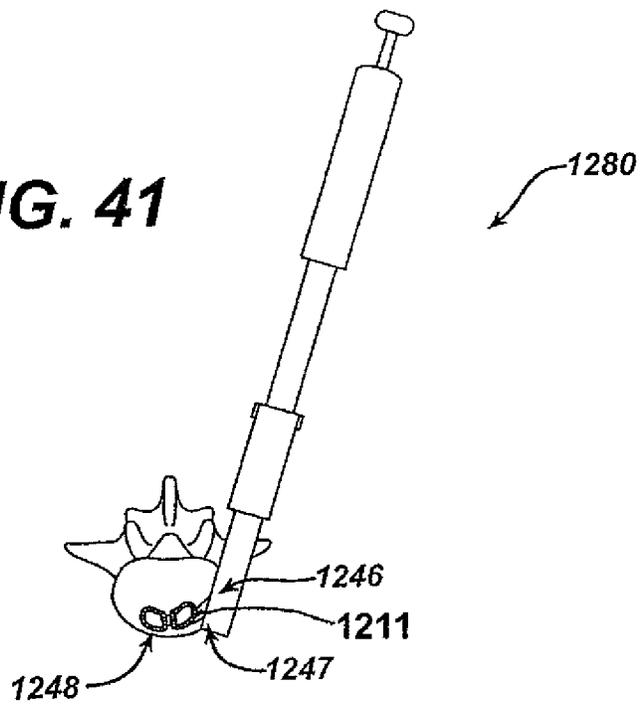


FIG. 42

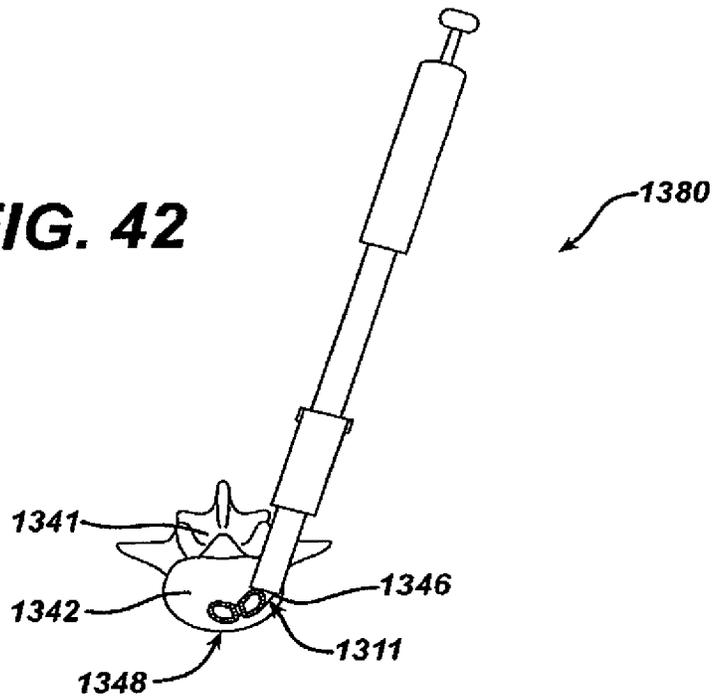


FIG. 43

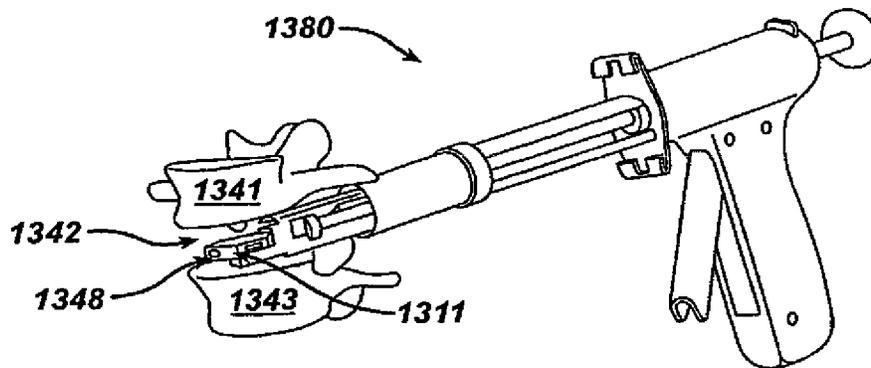


FIG. 44

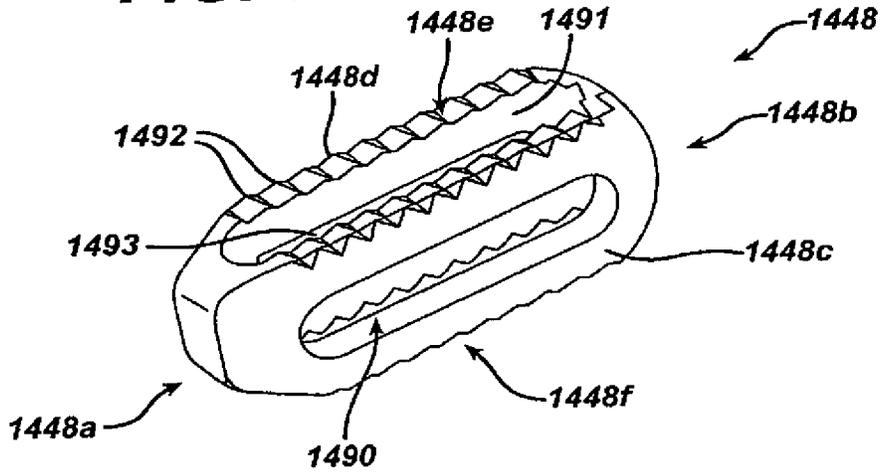


FIG. 45

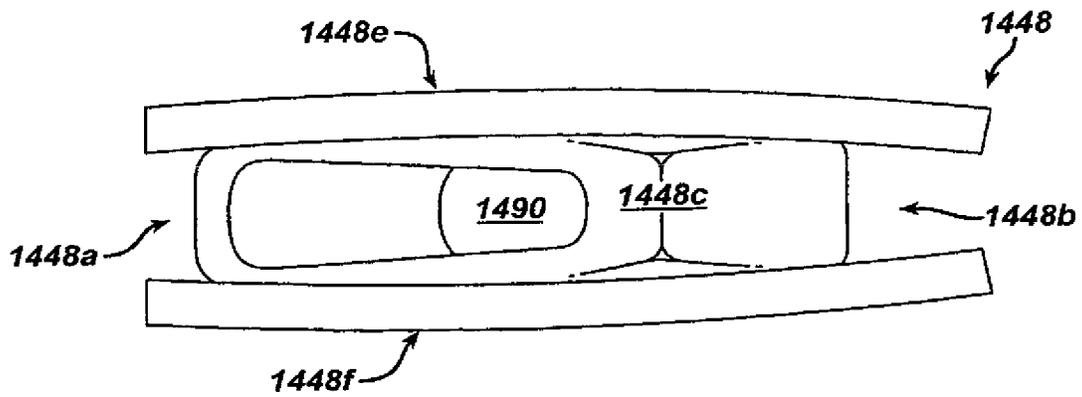


FIG. 46

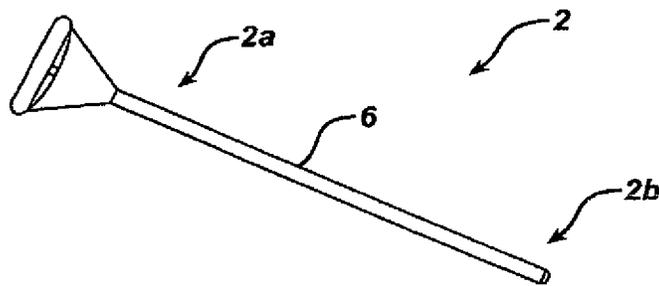
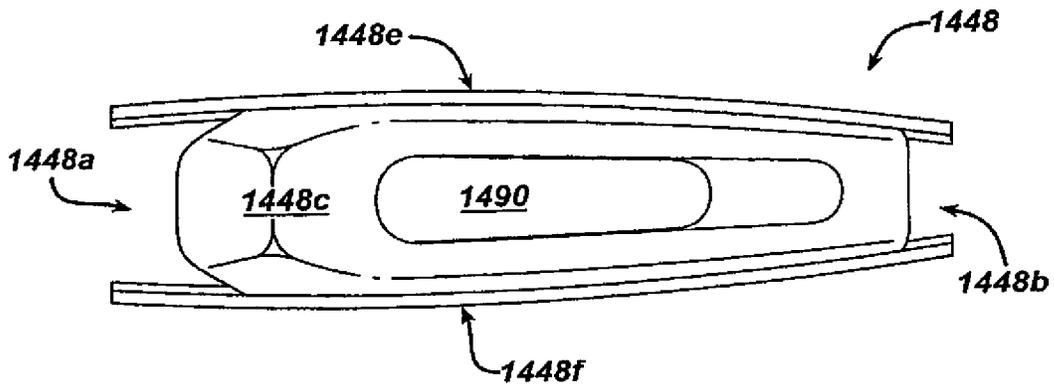


FIG. 47

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SYSTEMS AND METHODS FOR SPINAL SURGERY

RELATED APPLICATIONS

The present application is a divisional of U.S. application Ser. No. 10/579,146, filed Feb. 22, 2007, which is a U.S. national phase application filed pursuant to 35 U.S.C. 371 from PCT/US05/004136, filed Feb. 9, 2005, which claims the benefit of the filing date of U.S. Provisional Patent Application Ser. No. 60/543,030, filed Feb. 9, 2004, all of which are herein incorporated by reference.

FIELD OF THE INVENTION

The present invention relates to surgical instruments, and in particular to methods and devices for implanting spinal prostheses.

BACKGROUND

Spinal fusion surgeries, that is, the use of bone graft material to promote specific vertebrae to grow together into a solid and stable construct, are a common method of treating patients with severe back pain. For fusion to occur within the disc space, the surgeon must first remove the damaged disk material. Once the disk material is removed, the empty space left between the upper and lower vertebrae is distracted to relieve pressure from neural elements and to provide space for entry of surgical tools and/or implants. A bone graft, or interbody cage with bone, is then inserted into the empty disc space to promote bone growth from vertebral body to vertebral body. Recently, minimally invasive techniques have improved fusion procedures by causing less damage to tissue surrounding the damaged disk and allowing for faster recovery by the patient.

One drawback associated with current instruments used to perform spinal fusion surgery, especially minimally invasive surgery, is that they typically provide inadequate protection for sensitive nerve tissue surrounding the surgical site. The smaller access portals used in minimally invasive surgery allow sensitive tissue to be located very close to the surgical site. Further, using current instruments within these tight confines often impedes the surgeon's visibility, making the ultimate placement of the implant difficult.

Accordingly, there remains a need for improved surgical instruments, and in particular for surgical instruments used for implanting spinal prostheses.

SUMMARY

Disclosed herein are various methods and devices for implanting spinal prostheses. In one aspect, a surgical instrument system includes a distractor having a shaft, a paddle located at the distal end of the shaft, and a filler bar shaped to removably engage the shaft and paddle of the distractor. In an exemplary embodiment, when the filler bar is engaged to the distractor, the filler bar provides rigidity and torque strength so that the distractor can be inserted between adjacent vertebrae in a first orientation and rotated to distract adjacent vertebrae. A guide feature configured to mate with at least one of an implant or an implant inserter can extend along at least a portion of the shaft and the paddle, or alternatively, the paddle can further comprise at least one overhanging tab on at least one of the superior and inferior surfaces. Moreover, in a further exemplary embodiment, the surgical instrument sys-

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tem can comprise a minimally invasive access port through which the distractor is dimensioned to be placed.

In a further embodiment, at least one of the superior and inferior surfaces of the paddle can include a means for preventing migration of the distractor during distraction, such as, for example a bone engaging element or at least one expansion shoulder. The distractor paddle can also include an angled guide feature that is configured to guide an implant through a partial rotation to a desired angle. The angled guide feature can have a variety of configurations, such as an angled surface integral with a distal portion of the paddle, or, a movable shim that can be either retractable or a memory metal shim. The implant inserter can also include an angled distal end or an articulating implant holder operable to rotate an implant to a desired angle.

In a further aspect, a surgical instrument system includes a distractor having a shaft and a paddle located on the distal end of the shaft. The distractor paddle and the shaft can also present a guide surface for guiding the placement of an implant when the distractor is in the distraction orientation. The distractor paddle can also include an angled guide feature that is configured to guide an implant through a partial rotation to a desired angle. The angled guide features can have a variety of configurations, such as an angled surface integral with a distal portion of the paddle, or, a movable shim that can be either retractable or a memory metal shim. The distractor paddle can also include a first height dimension when presented in an insertion orientation and a second height dimension when rotated approximately 90 degrees to a distraction orientation, the second height dimension being greater than the first height dimension, the paddle having inferior and superior surfaces for contacting adjacent vertebrae in the distraction orientation. In a further embodiment, at least one of the superior and inferior surfaces of the paddle can include a means for preventing migration of the distractor during distraction, such as, for example a bone engaging element including at least one tooth or at least one expansion shoulder operable to extend beyond at least one of the inferior or superior surfaces so as to increase the second height dimension.

In a further embodiment, the surgical instrument system can also include an implant inserter having an angled distal end, the angle corresponding approximately to the angle provided on the angled guide feature or having an articulating implant holder operable to rotate an implant to a desired angle. Moreover, the surgical instrument system can also include guide features extending along the shaft and paddle configured for mating with at least one of an implant and an implant inserter to guide the insertion of an implant along the distractor. In a further embodiment, the surgical instrument system can include a filler bar shaped to removably engage the shaft and paddle of the distractor, wherein when the filler bar is engaged to the distractor, the filler bar provides rigidity and torque strength so that the distractor can be inserted between adjacent vertebrae in a first orientation and rotated to distract the adjacent vertebrae. The surgical instrument system can also include a minimally invasive access port through which the distractor is dimensioned to be placed.

In another aspect, a surgical instrument system includes a distractor having a shaft and a paddle located on the distal end of the shaft, the paddle further including inferior and superior surfaces configured for contacting adjacent vertebrae to define a distraction height. The surgical instrument system also includes at least one expansion shoulder operable to extend beyond at least one of the inferior or superior surfaces of the paddle so as to increase the distraction height. In one embodiment, the surgical instrument system can include a

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shim that can be slidable along a longitudinal axis of the distractor, and that can further include at least one expansion shoulder such that the distal movement of the shim causes the at least one expansion shoulder to increase the distraction height. The shim can also include an angled distal end such that distal movement of the shim causes the angled distal end to extend at an angle from a distal end of the paddle to form an angled guide. The system can further include a linkage assembly slidably connecting the paddle and the at least one extension shoulder, or, alternatively, a slidable shim having a shoulder for contacting the linkage assembly to effect changes in the distraction height. Moreover, the distractor paddle and the shaft can present a guide surface, which can optionally include a guide feature, for guiding the placement of an implant when the distractor is in the distraction orientation.

In still another aspect, the surgical instrument system can include an articulating implant inserter including a shaft, and an articulatable implant holding element located at the distal end of the shaft. The articulatable implant holding element can be operable from the proximal portion of the shaft to releasably hold an implant. Moreover, the surgical system can further include an implant having a connecting element that cooperates with the articulatable implant holding element to allow articulation of the implant to a desired angle. The implant connecting element can engage either an internal or external portion of the implant. Further, the articulatable implant holding element can include two sliding elements having distal implant impaction faces, such that the relative sliding of the sliding elements in a proximal-distal direction along the shaft selectively articulates the implant to a desired angle. The position of the handle can also act as a visual indicator for an angle through which the implant has been rotated.

In still another aspect, a surgical instrument system disclosed herein includes a means for distracting adjacent vertebrae, an implant, a means for inserting the implant into a space between the adjacent vertebrae upon insertion, and a means for rotating the implant to a desired angle between the adjacent vertebrae upon insertion. In certain embodiments, the means for distracting adjacent vertebrae includes two distraction paddles movable away from each other to distract adjacent vertebrae, or a distractor paddle having a first height dimension when presented in an insertion orientation and a second height dimension when rotated approximately 90 degrees to a distraction orientation, the second height dimension being greater than the first height dimension.

Moreover, the surgical instrument system can also include a shaft, a paddle located on the distal end of the shaft having inferior and superior surfaces configured for contacting adjacent vertebrae to define a distraction height, and at least one expansion shoulder operable to extend beyond at least one of the inferior or superior surfaces so as to increase the distraction height. While the means for insertion can vary, it can include a ratchet gun, or an articulating implant inserter operable to place the implant at a desired angle. The means for rotating the inserter can also vary can, and can include an articulating implant inserter or angled guide features located on a distal end of the means for distracting. Moreover, the implant can have a variety of configurations such as domed inferior and superior surfaces configured to correspond to surfaces of adjacent vertebra, or alternatively, a leading end having a bullet-shaped cross-sectional profile in at least two planes.

A method is provided in another aspect. In particular, a minimally invasive surgical method includes inserting a distractor assembly through a minimally invasive surgical access

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port and between adjacent vertebrae in an insertion orientation, the distractor assembly including a shaft, and a paddle located on the distal end of the shaft and a filler bar removably engaged to the shaft and the paddle of the distractor. The method can further include rotating the distractor assembly to a distraction orientation to distract the adjacent vertebrae, disengaging the filler bar from the shaft and paddle, and removing the filler bar through the minimally invasive access port while leaving the shaft and paddle in place to maintain a desired distraction of the adjacent vertebrae. In one embodiment, the distractor paddle includes a first height dimension when presented in an insertion orientation and a second height dimension when rotated approximately 90 degrees to a distraction orientation, the second height dimension being greater than the first height dimension. The paddle further includes inferior and superior surfaces for contacting adjacent vertebrae in the distraction orientation.

Moreover, the method can also include inserting an implant between the adjacent vertebrae using the shaft and paddle as a guide for placement of the implant. Alternatively, the method can include using a paddle with an angled guide element on its distal end, inserting the implant using the shaft and paddle as a guide for placement, and rotating the implant to a desired angle based on the angled guide element.

In a further aspect, an implant is provided. In one embodiment, the implant has a blended or "bullet-shaped" cross-sectional profile in at least two planes. In a further embodiment, the implant has a domed superior and/or inferior configured to conform generally to one or both adjacent vertebral end-plates at a predetermined angle of orientation of the implant. The implant can be combined with either a distractor that can guide the implant to the desired orientation (including a partial rotation of the implant) or an articulating insertion tool that can rotate the implant to the desired position.

BRIEF DESCRIPTION OF THE DRAWINGS

The invention will be more fully understood from the following detailed description taken in conjunction with the accompanying drawings, in which:

FIG. 1 is a side perspective view of one embodiment of a distractor assembly;

FIG. 2 is a side perspective view of one embodiment of the distractor of the distractor assembly of FIG. 1;

FIG. 3 is a side perspective view of the distractor assembly of FIG. 1 upon insertion into an intervertebral space;

FIG. 4 is a top perspective view of the distractor assembly of FIG. 1 upon insertion into an intervertebral space;

FIG. 5 is side perspective view of the distractor assembly of FIG. 1 upon insertion into an intervertebral space;

FIG. 6 is another side perspective view of the distractor assembly of FIG. 1 upon insertion into an intervertebral space;

FIG. 7 is a side perspective view of an implant being inserted into an intervertebral space using the distractor assembly of FIG. 1;

FIG. 8 is another side perspective view of an implant being inserted into an intervertebral space using the distractor assembly of FIG. 1;

FIG. 9 is a side perspective view of another embodiment of a distractor;

FIG. 10 is a side perspective view of an implant being inserted into an intervertebral space using the distractor of FIG. 9;

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FIG. 11 in another side perspective view of an implant being inserted into an intervertebral space using the distractor of FIG. 9;

FIG. 12 is a side perspective view of another embodiment of a distractor being inserted into an intervertebral space;

FIG. 13 is a side perspective view of an implant being inserted into an intervertebral space using the distractor of FIG. 12;

FIG. 14 is a side perspective view of another embodiment of a distractor;

FIG. 15 is a side perspective view of the distractor of FIG. 14 upon insertion into an intervertebral space;

FIG. 16 is another side perspective view of the distractor of FIG. 14 upon insertion into an intervertebral space;

FIG. 17 is a side perspective view of an implant being inserted into an intervertebral space using the distractor assembly of FIG. 14;

FIG. 18 is a side perspective view of another embodiment of a distractor upon insertion in an intervertebral space;

FIG. 19 is a side perspective view of the distractor of FIG. 18;

FIG. 20 is another side perspective view of the distractor of FIG. 18 upon insertion into an intervertebral space;

FIG. 21 is a side perspective view of another embodiment of a distractor;

FIG. 22 is a side perspective view of the distractor of FIG. 21 upon insertion into an intervertebral space;

FIG. 23 is another side perspective view of the distractor of FIG. 21;

FIG. 24 is a side perspective view of another embodiment of a distractor upon insertion into an intervertebral space;

FIG. 25 is another side perspective view of the distractor of FIG. 24 upon insertion into an intervertebral space;

FIG. 26 is another side perspective view of the distractor of FIG. 24 upon insertion into an intervertebral space;

FIG. 27 is a side perspective view of an implant being inserted into an intervertebral space using one embodiment of an inserter;

FIG. 28 is another side perspective view of an implant being inserted into an intervertebral space using the inserter of FIG. 27;

FIG. 29 is a side perspective view of the inserter of FIG. 27;

FIG. 30 is a side perspective view of another embodiment of an inserter;

FIG. 31 is another side perspective view of the inserter of FIG. 30;

FIG. 32 is a magnified view of the distal end of the inserter of FIG. 30;

FIG. 33 is another magnified view of the distal end of the inserter of FIG. 30;

FIG. 34 is a side perspective view of an implant being inserted into an intervertebral space using another embodiment of an inserter;

FIG. 35 is another side perspective view of an implant being inserted into an intervertebral space using the inserter of FIG. 34;

FIG. 36 is a side perspective view of another embodiment of an inserter;

FIG. 37 is a side perspective view of an implant being inserted into an intervertebral space using another embodiment of an inserter;

FIG. 38 is a side perspective view of another embodiment of a distractor assembly;

FIG. 39 is a side perspective view of the distractor assembly of FIG. 38 upon insertion into an intervertebral space;

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FIG. 40 is a side perspective view of another embodiment of a distractor assembly upon insertion into an intervertebral space;

FIG. 41 is another side perspective view of an implant being inserted into an intervertebral space using the distractor assembly of FIG. 40;

FIG. 42 is a side perspective view of an implant being inserted into an intervertebral space using another embodiment of a distractor assembly;

FIG. 43 is another side perspective view of the distractor assembly of FIG. 42 upon insertion into an intervertebral space;

FIG. 44 is a side perspective view of one embodiment of an implant;

FIG. 45 is a side perspective view of the implant of FIG. 44;

FIG. 46 is another side perspective view of the implant of FIG. 44; and

FIG. 47 is a side perspective view of one embodiment of a funnel.

DETAILED DESCRIPTION OF THE EXEMPLARY EMBODIMENTS

Disclosed herein are methods and devices for distracting adjacent vertebrae and/or inserting spinal implants during surgical procedures for repairing a patient's spine. In an exemplary embodiment, a distractor is disclosed that maintains the empty space between adjacent vertebrae following a discectomy, and that can removably mate with other surgical instruments, such as, for example, a filler bar, an implanting tool, or a funnel. In other embodiments of the present invention a distractor is disclosed having various features to assist in implanting a spinal prosthesis, such as, for example, an angled distal end and/or an expandable paddle. In another embodiment of the present invention, an articulating inserter is disclosed. Moreover, various implants and funnels are also disclosed herein. A person skilled in the art will appreciate that, while the methods and devices are described in connection with certain spinal procedures, the methods and devices disclosed herein can be used for a variety of surgical procedures.

Certain features and aspects of the present invention will now be described by reference to the distractor assembly and associated elements illustrated in FIGS. 1 to 8, which illustrate a distractor assembly system and method for inserting a spinal prosthesis.

FIG. 1 illustrates one embodiment of a distractor assembly 10 disclosed herein having a distractor or guide arm 12, a guide filler bar 26, and a modular handle 16. While the distractor 12 can have a variety of configurations that enable it to maintain the space between adjacent vertebrae following a discectomy, as shown in FIG. 2, the distractor 12 has proximal and distal ends 12a, 12b with an elongate shaft 14 extending therebetween. Attached to the proximal end 12a of the distractor 12 is a handle 16 (or a portion thereof) for gripping by the surgeon. While the handle 16 can be either fixedly or removably attached, in an exemplary embodiment, the handle 16 is removably attached to the shaft 14 by any means known in the art, such as, for example, a screw or a spring plunger, so that the surgeon can remove it to achieve increased visibility to the surgical site.

Extending distally from the handle 16 is an elongate shaft 14. While the shaft 14 can have a variety of sizes, it should have a diameter that, upon insertion into the intervertebral space, allows sufficient space for the insertion of other surgical tools, such as a filler bar or an inserter for example, as well as an implant. Additionally, the shaft 14 can have a variety of

shapes, such as circular, oval, rectangular or square. As shown, the shaft **14** is rectangular and generally flat.

The shaft **14** can also have a variety of configurations that allow for mating with another surgical instrument, such as, for example, a filler bar, an inserter, a funnel, or any other instrument used in the implanting of a spinal prosthesis. In an exemplary embodiment, the shaft **14** can have a guide feature **18** such as a tooth or groove that can mate with a corresponding guide feature on another surgical instrument. The guide feature **18** can be formed either throughout the entire length of the shaft **14** or on a partial length thereof. The guide feature **18** can also have a variety of configurations depending upon the mating features of the corresponding surgical instrument. For example, in one embodiment, the guide feature **18** can be protrude from the shaft **12**, or, alternatively, the guide feature **18** can be recessed within the shaft **12**. The guide feature **18** can also have a variety of shapes, however in an exemplary embodiment, the guide feature **18** has a C-shape with two opposed sides that are either straight or curved. In addition, outer features, including the cross-sectional shape of the shaft itself, can form mating or guiding features.

Attached to the distal-most end of the shaft **14** is a distracting paddle **22** that, upon insertion into the cavity, can be rotated to distract adjacent vertebrae to maintain the integrity of the cavity between them. As shown, paddle **22** has proximal and distal ends **22a**, **22b** connected by superior and inferior sides **22c**, **22d** and having a front or guiding face **22e** and a back face **22f**. While paddle **22** can have a variety of shapes, such as rectangular, circular or oblong, the illustrated paddle **22** is generally rectangular with rounded corners. The paddle **22** can also have a variety of sizes to provide a desired level of distraction, so long as it has a width that is less than the diameter of any access portal into the intervertebral space. In an exemplary embodiment, the paddle **22** has a width that is less than about 19 mm, and more preferably about 7 mm. The paddle may also be shaped so as to provide an angle between the inferior and superior sides to match a desired angle of distraction.

The paddle **22** can have a variety of additional features to assist the surgeon with distraction, which can be used alone or in combination with one another. In addition to those features discussed in more detail below, in one embodiment, the distal end **22b** of the paddle **22** can be arcuate to allow for easier insertion into the intervertebral space **42**. In addition, the superior and/or inferior sides **22c**, **22d** can have various geometries to enhance the distraction of the intervertebral space **42**, such as laterally extending surfaces that provide a larger surface area to contact the vertebrae. The back side **22f** can also be dome-shaped to aid the surgeon in minimizing damage to the neural tissue surrounding the intervertebral space **42**. One of superior and inferior sides **22c**, **22d** can also be provided with a bone engaging element such as one or more teeth to prevent migration of the paddle during distraction.

Additionally the paddle **22** can have a variety of features to assist the surgeon with positioning of the implant **48** within the intervertebral space **42**. In addition to those features discussed in more detail below, guide surface **22e** of the paddle **22** can include at least one guide feature such as guide feature **18** extending from the shaft **14** to engage a corresponding element in an implant or implant inserter. Alternatively, the implant or implant inserter can be guided by a flat guide surface **22e** or by external features of the shaft **14**.

As noted above and referring back to FIG. 1, a filler bar **26** can be removably mated to the distractor **12** to provide rigidity and torque strength to the distractor **12** during insertion into the cavity **42** and distraction of the adjacent vertebrae. As

shown in FIG. 1, the filler bar **26** has proximal and distal ends **26a**, **26b** with a shaft **28** extending therebetween. The proximal end **26a** can have a variety of configurations to assist the surgeon with placement and removal of the filler bar **26** from the distractor **12**, however as shown the filler bar **26** has a T-shaped handle **30**. Alternatively, the proximal end of the filler bar can include a portion of a handle that can mate with a corresponding handle portion on a distractor, such that when mated together, a complete handle is formed. While the handle portions can mate to one another in a variety of ways, in an exemplary embodiment, the handle portions are mated together by a spring lock mechanism.

Extending distally from the T-shaped handle **30** is an elongate shaft **28**. While the shaft **28** can have a variety of sizes, as shown it has a diameter that is less than the diameter of the distractor. Additionally, the shaft **28** can have a guide feature **32** that corresponds to the guide feature **18** on the distractor **12**. That is, the guide feature **32** can be either protruding or recessed, and have a variety of shapes, such as C-shaped with two opposed sides that can be either straight or curved. While the guide feature **32** can be formed throughout the entire length of the shaft **28** or on a partial length thereof, as shown, the groove **32** is formed throughout the entire length of the shaft **28**.

Fixedly attached to the distal most end of the shaft **28** is a stabilizing plate **34**. The plate **34** can have any size so long as it is able to fit within the intervertebral space alongside the distractor **12**, however in an exemplary embodiment the plate **34** is shaped such that it can nest within the distracting paddle **22**, and in particular, within the laterally extending portions of superior and inferior surfaces **22c**, **22d**. Thus, in an exemplary embodiment, the plate **34** has width that is slightly smaller than the distracting paddle **22** and complementary in shape thereto.

In a further embodiment, an implant inserter can be used with the distractor to form a distraction and insertion system. Generally, the inserter can be similar to inserters known in the art, as well as the inserter **46** shown in FIGS. 7 and 8. As shown in FIGS. 7 and 8, the inserter **46** has proximal and distal ends **46a**, **46b** with a shaft **52** extending therebetween. While the proximal end **46a** can have a variety of configurations, in an exemplary embodiment it can have a handle (or a portion thereof) fixedly or removably attached thereto.

Extending distally from the handle of the inserter **46** is an elongate shaft. While the shaft **52** can have a variety of configurations, the shaft **52** can also optionally include a guide feature **50** that corresponds to the guide feature **18** on the distractor **12**, such that the inserter **46** can be mated to the distractor **12**. Thus, depending upon the configuration of the guide feature **18** on the distractor **12** the guide feature **50** on the inserter **46** can be either protruding or recessed, and can be, for example, C-shaped with two opposed sides that are either straight or curved. Moreover, the guide feature **50** on the inserter **46** can be formed either throughout the entire length of the shaft **52** or on a partial length of the shaft **52**. Alternatively, the inserter may simply be guided by a flat surface on the shaft **14** and/or paddle **22** on the distractor **12** or by an external feature of the shaft **14** such as, for example, its superior and/or inferior surfaces. Removably mated to the distal most end of the shaft **52** is an implant **48**, various embodiments of which will be discussed below.

In use, as shown in FIGS. 3 to 8, the distraction assembly **10** is inserted into the intervertebral space **42** (that is, the space between superior and inferior vertebrae **41**, **43**) following the excision of disk material. The distraction assembly **10** is then rotated approximately 90° such that the paddle **22** is substantially perpendicular to the superior and inferior verte-

brae **41**, **43**, so as to enlarge and/or maintain a desired space within the cavity **42** by the force applied to the vertebrae by superior and inferior surfaces **22c**, **22d** during rotation. One skilled in the art will appreciate that where the instruments are used in a minimally invasive surgical procedure, such as shown in FIGS. **5** to **8**, access to the surgical site can be gained using an access port such as cannula **51**.

Following distraction of the cavity **42**, the filler bar **26** can be removed from the distractor **12** to decrease the amount of space that the assembly **10** requires in order to make room for further tools and/or implants as well as to improve the surgeon's ability to visualize the cavity. As shown in FIGS. **7** to **8**, an inserter **46** can then be slidably guided by the distractor **12**. Specifically, the surgeon slidably mates the guide features **18**, **32**, if any, on the distractor **12** and the inserter **46** to one another, and the inserter **46** is slid distally along the distractor **12** into the intervertebral space **42**. Once the inserter **46** is placed within the cavity **42**, the implant **48** can then be maneuvered so as to achieve the desired orientation.

The distractor assembly disclosed herein can also optionally include a measurement system (not shown). The measurement system can be any indication that allows a surgeon to determine the depth of placement of the distractor, a trial implant or the implant. In an exemplary embodiment, however, the measurement system is formed along the entire length of the shafts of the distractor, filler bar, and/or inserter, or only on a portion thereof. In addition, the distractor can include at least one colored band so as to color code for the height of the distraction paddle that the distractor can be matched to a similarly color coded trial implant and/or implant so that a surgeon can readily ensure that all are of the same height.

As noted above, the distractor assemblies disclosed herein can have a variety of features to assist in implanting the spinal prosthesis, such as those features shown in FIGS. **9** to **43**. Specifically, FIGS. **9** to **26** illustrate distractors having features that assist a surgeon in inserting an implant into an intervertebral space at a desired angle. At the outset it should be noted that the distractor of the embodiments described below can have features and methods of use similar to those of distractor **12** discussed above.

FIGS. **9** to **11** illustrate one embodiment of a distractor **112** that includes a paddle **122** having an angled distal end **122b**, and thus providing an angled guide surface **122c**. Many times, an implant is designed for placement at a certain angle of trajectory between the adjacent vertebrae and/or a surgeon chooses a particular angle of placement in order to achieve desired fusion characteristics. Minimally invasive approaches to the disk space provide well documented advantages, however, establishing a minimally invasive access portal while sparing sensitive nerve tissues from contact and possible damage requires approach angles to the disk space that may not match the desired angle of placement of the implant. For example, a typical TLIF approach may take a 35° angle (plus or minus depending on the anatomy of a particular patient) while the desired angle for placement of the implant may be 45°. Providing an angled distal end **122b** on the distractor paddle **122** allows the surgeon to carefully guide the implant during insertion to the desired angle with a reduced chance of contacting sensitive nerve tissue. While the distal end **122b** of the paddle **122** can have a variety of angles as desired by the surgeon, in the illustrated embodiment, the distal end **122b** of the paddle **122** has an angle of about 20°.

Paddle **122** can further include opposed overhanging tabs **123a**, **123b** and a curved distal end **122b**. The overhanging tabs **123a**, **123b** can be any configuration that can serve as a guide for the implant **148**, however, as shown, the overhang-

ing tabs **123a**, **123b** are rectangular and extend horizontally from the guide surface **122c** of the paddle **122**.

In use, as an inserter (such as inserter **146**) is slid distally along the shaft **114** of the distractor **112**, the overhanging tabs **123a**, **123b** of the paddle **122** can slidably engage the outer edge surfaces of the implant **148**. Once engaged, the implant **148** is guided along the length of the paddle **122**. As the implant **148** approaches the distal end **122b** of the paddle **122**, the angled distal end **122b** urges the implant **148** into the desired orientation within the intervertebral space **142**.

FIGS. **12** to **13** illustrate another embodiment of an angled distractor **212** that includes a shape memory metal shim **211**. While the metal shim **211** can have any configuration to allow for the angled insertion of an implant **248**, as shown the memory metal shim **211** is provided as a separate element from the distractor **212** that is placed along the side of the shaft **214** and paddle **222** of the distractor **212**. Shim **211** can be held flat to the shaft **214** and/or paddle **222** of the distractor by one or more guide elements **213**.

In use, extension of the shim **211** distally along the paddle **222** (generally by pushing on a proximal end or feature of the shim) beyond the guide elements **213** causes the shim to return to a curved shape. The angle of curvature of the shape memory metal shim **211** can be any angle that allows a surgeon to implant an spinal prosthesis into an intervertebral space **242**, however in an exemplary embodiment, the curve of the shim **211** has an angle of about 20°. An implant **248** is then inserted into the intervertebral space **142** and, upon contact with the shim **211**, is directed towards the desired placement angle within the intervertebral space **242**. The shim **211** can also be retracted/straightened so that retraction of the distractor **212** does not displace the implant and so that retraction of the distractor does not disturb sensitive tissue.

The shim **211** can be made of any biocompatible material known to have shape memory or superelastic properties such as, for example, the NITINOL (an acronym for Nickel Titanium Naval Ordnance Laboratory) family of intermetallic materials, which contain a nearly equal mixture of nickel (55 wt. %) and titanium. One skilled in the art will appreciate that the ability of the shim **211** conform to the shape of the distractor **212** during insertion and then retain its curved shape once it is placed within the intervertebral space **242** allows for a reduced profile for insertion and retraction through a minimally invasive surgical access point.

FIGS. **14** to **17** illustrate an alternate embodiment of a distractor **312** that includes a paddle **322** having a shape memory metal shim **311** similar to metal shim **211** (described above), as well as extension shoulders **333a**, **333b**. While the extension shoulders **333a**, **333b** can have a variety of configurations, in an exemplary embodiment, they are slidably located on the paddle **322** and extendable from the superior and inferior sides thereof. However, in an alternate embodiment (not shown), a single extension shoulder can be formed on the paddle.

In use, following insertion into an intervertebral space **342** and rotation of the paddle **322** to a distracting position, the distal movement of the shim **311**, and in particular, contact between driving shoulders **313** on the shim **311** and the extension shoulders **333a**, **333b**, drives the extension shoulders **333a**, **333b** upward and downward, respectively, to further distract the intervertebral space **342**. While extension shoulders **333a**, **333b** can increase the height of the paddle **322** by any amount as desired by the surgeon to achieve and maintain a desired level of distraction of intervertebral space **342**, in an exemplary embodiment, the paddle has a height of approximately 7 mm and extension shoulders **333a**, **333b** increase the diameter of the paddle **322** by an amount up to approximately

4 mm. By providing at least some of the distraction height by extension rather than rotation, a more sure placement of the distractor can be achieved with less movement within the cavity during distraction. Moreover, following extension of the extension shoulders **333a**, **333b**, the memory metal shim **311** extends beyond the distal end **322b** of the paddle **322**, and retains its curved shape, such that the surgeon can place the implant **348** into the cavity **342** at a desired angle.

FIGS. **18** to **20** illustrate an alternate embodiment of a distractor **412** having an internal shim **409**, as well as extension shoulders **433a**, **433b**. While the internal shim **409** can be formed in a variety of ways, as shown the internal shim is **409** is formed within a sheath **407** surrounding the shaft **414** of the distractor **412**. The internal shim **409** can also include an expansion mechanism such that, in use, and similar to the memory metal shim **211** discussed above, the internal shim **409** drives the extension shoulders **433a**, **433b** upward and downward, respectively, as the surgeon desires.

Alternatively, as shown in FIGS. **21** to **23**, the expanding shoulders **533a**, **533b** of a distractor **512** can be driven by an internal shim **509** having a linkage assembly **505**. While the linkage assembly **505** can be formed in a variety of ways, as shown the linkage assembly **505** is also formed within a sheath **507** surrounding the shaft **514** of the distractor **512**. In use, similar to the embodiment above, the internal shim **509** can drive the linkage assembly **505** to control the height of the extension shoulders **533a**, **533b** as desired.

FIGS. **24** to **26** illustrate another embodiment of a distractor **612** having an inserter arm **660** for positioning the distractor. Distractor **612** can include an internal shim **609** and extension shoulders **633a**, **633b**, similar to those as discussed above. The inserter arm **660** can be removed after placement of the distractor **612**, and a cable **662** is left behind extending distally from the distractor **612**.

In use, the shim **609** drives the extension shoulders **633a**, **633b** to set a height adjustment, similar to that as described above with respect to extension shoulders **333a**, **333b**. Once the cavity **642** is distracted to the desired height, the inserter arm **660** can be slidably removed from the cable **662**, resulting in the cable **662** extending out of the intervertebral space **642**. The cable **662** can then either be removed or used as a guide for other surgical instruments. One skilled in the art will further appreciate that the shim **609** can also optionally include a sliding support **613** that can be slid along the shaft **614** of the distractor **612** to lock the extension shoulders **633a**, **633b** in place, and help secure the distracted height of the cavity **642**.

The cable **662** can be made from a variety of materials depending upon its desired use by the surgeon. For example, if the surgeon desires the cable to be used as a guide for future instruments or procedures, the cable can be made of any desirable surgical material of sufficient guide strength.

FIGS. **27** to **36** illustrate implant inserters having features that assist a surgeon in inserting an implant into an intervertebral space at a desired angle. At the outset it should be noted that the inserters of the embodiments described below can have features and can be used in a manner similar to that of inserter **46**, discussed above. Moreover, depending upon the particular surgical assembly, the shafts of the inserters in the embodiments described below may or may not include a guide feature for slidably engaging with another surgical instrument.

FIGS. **27** to **29** illustrate one embodiment of an inserter **746** that includes a hinge pivot joint **770** and a linkage mechanism **772**. While the hinge pivot joint **770** and the linkage mechanism **772** can have a variety of configurations to drive the implant **748** to desired angulations, in one embodiment, the

hinge pivot joint **770** and a linkage mechanism **772** are formed at the distal end **746b** of the inserter **746**, and located external to the shaft **752** thereof. Alternatively, the hinge pivot joint **770** and the linkage mechanism **772** can be formed within a pathway (not shown) contained within the shaft **752** of the inserter **746**. The inserter **746** can also include a variety of means by which the surgeon can control the hinge pivot joint **770** and the linkage assembly **772**, such as, for example, a spring bias built into or placed on the pivot joint, and control the movement in response to the bias by proximal or distal movement of the linkage assembly. Thus, in use, the surgeon can maneuver the linkage mechanism such that the hinge pivot joint **770** and a linkage mechanism **772** cooperate to place the implant **748** at a desired angle.

FIGS. **30** to **33** show another embodiment of an inserter **846** that includes mating impaction arms **878a**, **878b** to rotate the implant **848** to the desired orientation. While the mating impaction arms **878a**, **878b** can rotate the implant **848** in a variety of ways, as shown, the mating impaction arms **878a**, **878b** include a mating face **879** that allows high impaction forces on the implant **848** by maintaining a high surface area of contact. Handle or knob **883** is rotated to drive the impaction arms relative to each other so as to rotate the implant, and the position of the knob can indicate the angle to which the implant is rotated as can be seen in the differential angulations illustrated by comparing FIGS. **30** and **31**.

The mating face **879** can have any configuration, but preferably allows for a high surface area contact with the implant **848**, however in an exemplary embodiment the mating face **879** includes an adjustable driving mechanism having a movable protrusion **881** mated to the cavity of an implant **848**. FIG. **32** illustrates an up close view of the translating impaction arms described above for an inserter that allows for implant rotation during insertion. The implant **848** includes an internal cavity **885** in which a inserter driver **881** mates while allowing the implant to rotate. The implant **848** is loaded by inserting the driver **881** into the implant cavity **885** and rotating the driver 90 degrees as illustrated in FIG. **34** (loading position) and FIG. **33** (insertion position). The implant **848** can be removed from the inserter by rotating the implant 90 degrees, in the reverse of the loading step for example.

FIGS. **34** to **35** illustrates another embodiment of an inserter **946** that allows cable rotation of implant **948** with respect to vertebra **941** by a cable **962** that is linked to the implant **948**. Inserter shaft **952** permits rotation of the implant in a hinge-like manner when the cable **962** is operated by the surgeon to drive the rotation. When the inserter shaft **952** is removed, the cable **962** must be disengaged from at least one of the implant **948** (in which case the cable **962** is removed with the shaft **952**) or the shaft **952** (in which case the cable **962** is left behind with the implant **948**). If the cable **962** is left behind, it can be formed, for example, from a bioabsorbable material.

FIG. **36** illustrates an exemplary embodiment of an implant driver **1346** that can be used with inserter **946** to permit rotation of the implant **1348**. The implant **1348** includes an external boss feature **1387** that is held between two inserter tabs **1388a**, **1388b**. The inserter tabs **1388a**, **1388b** can have a variety of configurations, however in an exemplary embodiment, they include an inserter tab movement mechanism that allows a surgeon to adjust the angulation of the implant **1348**, for example by using cable **962** from the embodiment of FIGS. **34** and **35**. In one sense, external boss feature **1387** and tabs **1388a**, **1388b** are the inverse of cavity **885** and inserter driver **881** from the embodiment of FIGS. **32** and **33**. Both

configurations can allow angulation of the implant, but by contact with external and internal surfaces of the implant respectively.

In other embodiments of the present invention, such as those shown in FIGS. 37-43, the inserter can have a controlled insertion feature to allow incremental insertion and placement of an implant 1048, such as, for example a ratchet gun. Such a gun may have a variety of configurations known in the art, as shown in FIG. 37, the ratchet gun inserter 1080 can include a flexible sheath 1081 to protect the neural tissue from injury during insertion into the intervertebral space 1042 of implant 1048 through minimally invasive access port 1082. Ratchet gun inserter 1080 can further include a flexible inserter connection 1085, such as metal laser cut tubing or helical springs, can be used to allow for implant rotation as described in other embodiments.

FIGS. 38 and 39 show one embodiment of a ratchet gun 1180 that includes distraction paddles 1184a, 1184b. While the distraction paddles 1184a, 1184b can have a variety of configurations known in the art, in an exemplary embodiment, they extend from the distal most end of the ratchet gun and are shaped and sized such that they fit against the inner surfaces of the superior and inferior vertebrae 1141, 1143. As this embodiment includes paddle distractors, inserter 1180 is not intended to be guided by a paddle distractor as with embodiments described above.

In use, the surgeon inserts the ratchet gun inserter 1180 into the intervertebral space 1142 and squeezes the handle of the gun (likely repeatedly) so that implant 1148 slides between distraction paddles 1184a, 1184b and extends the paddles away from each other to distract the intervertebral space 1142.

As further shown in FIGS. 40 and 41, a ratchet gun inserter 1280, similar to ratchet gun inserter 1180, can include a rotating inserter 1247 that can have any configuration as described herein (above in FIGS. 27 to 36). Alternatively, as shown in FIGS. 42 and 43, the ratchet gun 1280 can include a memory metal shim 1211, such as that described in FIGS. 12 and 13 above to allow insertion of an implant at a desired angulation.

A variety of implants can be used with the instruments disclosed above, such as, for example, the implants disclosed in U.S. Pat. No. 4,743,256 to Brantigan, U.S. Pat. No. 4,834,757 to Brantigan, U.S. Pat. No. 4,878,915 to Brantigan, U.S. Pat. No. 5,192,327 to Brantigan, U.S. Pat. No. 5,425,772 to Brantigan, U.S. Pat. No. 5,716,415 to Steffee, U.S. Pat. No. 5,984,922 to McKay, U.S. Pat. No. 6,245,108 to Biscup, as well as the implants disclosed in FIGS. 44 to 46. While the implants can have a variety of configurations, in an exemplary embodiment, as shown in FIG. 44, the implant 1448 has opposed front and back ends 1448a, 1448b and parallel side surfaces 1448c, 1448d. Upper and lower surfaces 1448e, 1448f that engage the adjacent vertebrae extend between the side surfaces 1448c, 1448d, and such a cavity 1493 is formed within the center of the implant 1448.

The back end 1448b of the implant 1448 can have a profile and features to mate with an inserter instrument such as are known in the art or as described above. Additionally, at least one slot 1490 for vascularization can be formed in at least one of the parallel side surfaces 1448c, 1448d and/or the upper and lower surfaces 1448e, 1448f. While the slots 1490 can have a variety of shapes, e.g., circular, ovalar, spherical, as shown the slot is ovalar. Additionally, at least one of the parallel side surfaces 1448c, 1448d and/or the upper and lower surfaces 1448e, 1448f has a plurality of pyramid-shaped teeth 1492 formed thereon and extending outward to

contact the superior and inferior vertebral surfaces 41, 43 and to resist retropulsion of the implant during or after insertion.

Further, as shown in FIG. 44, the front end 1448a of the implant 1448 can have a geometry that allows for entry into the disk past neural elements and for easier manipulation in the disk space. While this geometry can have a variety of forms, in an exemplary embodiment, it is a bullet-shaped profile, with a bulleted front profile in at least one, but preferably two planes. One skilled in the art will appreciate that the implant having a bullet formed in two planes is able to more effectively distract the vertebrae and neural tissue.

Further, the interior of the parallel side surfaces 1448c, 1448d and/or the upper and lower surfaces 1448e, 1448f can include a plurality of ridges 1491 formed thereon for the maximum retention of the bone graft material within the cavity 1493. While the ridges 1491 can have a variety of shapes, in an exemplary embodiment the ridges 1491 can be slots that extend vertically along the interior surface of the parallel side surfaces 1448c, 1448d and/or the upper and lower surfaces 1448e, 1448f. Alternatively, the ridges 1491 can be slots that horizontally extend along the inner surface of the parallel side surfaces 1448c, 1448d and/or the upper and lower surfaces 1448e, 1448f. Moreover, in an additional embodiment, the inner surfaces of the parallel side surfaces 1448c, 1448d and/or the upper and lower surfaces 1448e, 1448f can include both vertically and horizontally extending ridges 1491.

In addition, as shown in FIGS. 45 to 46, upper surface 1448e of the implant 1448 can have a dome structure formed thereon. While the dome can have a variety of configurations, in an exemplary embodiment the dome is angled such that it corresponds to the shape of the superior and inferior vertebrae at a desired angle of rotation. One skilled in the art will appreciate that this implant allows for insertion at an angle that is approximately 35° off of the midline of the vertebrae.

The materials used for forming the implants disclosed herein can vary. One preferred material from which the implant can be made is a carbon fiber reinforced polymer. Other materials from which the implants can be made include metals, metal alloys, biologically compatible polymers, allograft bone, and combinations of these materials. Examples of suitable polymers include polyether sulfone, polycarbonate, and bioabsorbable polymers, and examples of suitable composites include carbon fiber reinforced polymers. Examples of suitable metals include titanium, stainless steel, tantalum, cobalt chromium, aluminum, and combinations thereof.

As noted above a graft material funnel 2 can also be used with the distractor assembly disclosed herein. As shown in FIG. 47, the graft material funnel 2 has proximal and distal ends 2a, 2b connected by a shaft 6. The proximal end 2a can have a variety of features known in the art to contain bone graft material to be siphoned into the implant. While the shaft 6 can have a variety of configurations, such as elongate or curved, as shown it is curved. One skilled in the art will appreciate that the curved shape of the shaft allows rotation to implant graft material to a desired location. Additionally, while the shaft 6 can be made from a variety of materials, in an exemplary embodiment, the shaft 6 is made from a material that allows for the shaft diameter to have some flexibility, such that the graft material can be introduced into the funnel 2 without clogging.

The instruments described herein can be made from any suitable surgical grade material, including surgical grade stainless steel, titanium, aluminum, tantalum, cobalt chromium, plastics, and combinations and copolymers thereof.

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One skilled in the art will appreciate further features and advantages of the invention based on the above-described embodiments. Accordingly, the invention is not to be limited by what has been particularly shown and described, except as indicated by the appended claims. All publications and references cited herein are expressly incorporated herein by reference in their entirety.

What is claimed is:

1. A surgical instrument system, comprising:
 an articulating implant inserter including
 a shaft; and
 an articulatable implant holding element having a hinge pivot joint and located on a distal end of the shaft, the articulatable implant holding element being operable from a proximal portion of the shaft to releasably hold an implant; and
 an implant having a connecting element that cooperates with the articulatable implant holding element to allow articulation of the implant to a desired angle upon operation of the implant holding element.
2. The system of claim 1, wherein the implant connecting element is internal to the implant.
3. The system of claim 1, wherein the implant connecting element is external to the implant.
4. The system of claim 1, wherein the articulatable implant holding element includes two sliding elements having distal implant impaction faces, the implant holding element being operable from a proximal handle to provide relative sliding in a proximal-distal direction along the shaft to selectively articulate the implant to a desired angle.

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5. The system of claim 4, wherein the position of the handle acts as a visual indicator for an angle through which the implant has been rotated.

6. The system of claim 1, wherein the implant is a fusion cage.

7. A surgical instrument system, comprising:
 an articulating implant inserter including
 a shaft; and
 an articulatable implant holding element located on a distal end of the shaft, the articulatable implant holding element being operable from a proximal portion of the shaft to releasably hold an implant; and

an implant having a connecting element that cooperates with the articulatable implant holding element to allow articulation of the implant to a desired angle upon operation of the implant holding element;

wherein the articulatable implant holding element includes two sliding elements having distal implant impaction faces, the implant holding element being operable from a proximal handle to provide relative sliding in a proximal-distal direction along the shaft to selectively articulate the implant to a desired angle; and

wherein the position of the handle acts as a visual indicator for an angle through which the implant has been rotated.

8. The system of claim 1, wherein the implant connecting element is internal to the implant.

9. The system of claim 7, wherein the implant is a fusion cage.

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